

Preparation of Monodisperse Giant Unilamellar Anchored Vesicles Using Micropatterned Hydrogel Substrates

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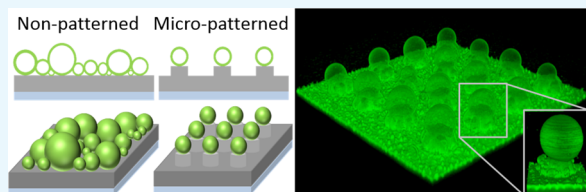
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S Supporting Information

ABSTRACT: Giant unilamellar vesicles (GUVs) are model membrane systems consisting of a single lipid bilayer separating an inner lumen from the outer solution, with dimensions comparable to that of eukaryotic cells. The importance of these biomimetic systems has recently grown with the development of easy and safe methods to assemble GUVs from complex biorelevant compositions. However, size and position control is still a key challenge for GUV formation and manipulation. Here, a gel-assisted formation method is introduced, able to produce arrays of giant unilamellar anchored vesicles (GUAVs) with a predetermined narrow size distribution. The approach based on micropatterned gel substrates of cross-linked poly(*N*-isopropylacrylamide) allows performing parallel measurements on thousands of immobile unilamellar vesicles. Such power and flexibility will respond to the growing need for developing platforms of biomimetic constructs from cell-sized single bilayers.



1. INTRODUCTION

Model lipid membranes are essential tools for unraveling the mechanisms that drive complex biological processes at the level of cell membranes.^{1,2} In the family of available model lipid platforms, giant unilamellar vesicles (GUVs) strike as a prominent member.³ These cell-sized vesicles are composed of a single bilayer that separates an enclosed volume from the outer solution. Giant vesicles were first used to study the intrinsic physical and chemical properties of membranes: permeability, lipid mobility, mechanical behavior, and phase transformations.^{4,5} Today, they are employed not only in biophysics and biology but also in physical chemistry in quests for understanding the origin of life and in several application-driven fields such as microreactor synthesis or drug delivery.^{6–8}

The first methods available for the formation of GUVs were often limited to a restricted variety of lipids. Over the past decade, many new strategies were developed for self-assembling giant vesicles from increasingly complex compositions of lipids and other (bio)macromolecules.⁸ The concomitant development of new methods for their observation and micromanipulation has now brought giant vesicles to the central stage of studies related to lipid bilayers. Here, the widening community of users calls for accuracy and predictability in the size distribution, for simplification of the methods for position control and for progress in the statistical power of the analysis performed on individual GUVs.

In this paper, we address these challenges by combining the advantages of gel-assisted methods for GUV formation with

the precision and flexibility offered by gel micropatterning. Although photolithography and microcontact printing techniques have been previously used to attempt size control of GUVs, these attempts lacked the advantages of gel-growing methods and did not achieve good vesicle unilamellarity by gentle hydration or required electrical fields to induce unilamellar vesicle formation.^{9–15} Photolithographic masks on an agarose gel circumvented some of these difficulties but controlled only the spatial distribution of spread lipids, leading to vesicle size polydispersity above 30%.¹⁶ Recently, giant lipid vesicles were prepared also on PDMS¹⁷ and Si¹⁸ microwell arrays. As we will show here by appropriate patterning and cross-linking of the gel films, one can generate arrays of thousands of monodisperse giant unilamellar vesicles anchored on the substrate. We coin this new platform as giant unilamellar anchored vesicles (GUAVs) and demonstrate its advantages by performing fluorescence correlation spectroscopy (FCS) experiments on the immobilized vesicles and parallel measurements of membrane area changes induced by oxidative stress.

2. RESULTS AND DISCUSSION

2.1. Preparation of Micropatterned Hydrogel Layers.

Our strategy for preparation of micropatterned, anchored

Received: April 1, 2019

Accepted: May 16, 2019

Published: May 29, 2019

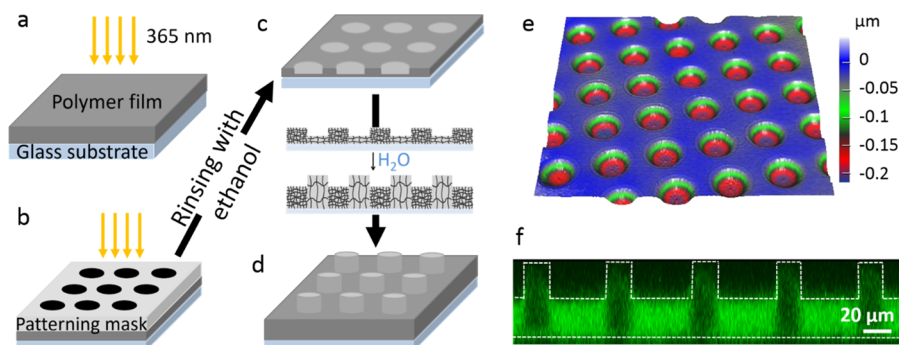


Figure 1. Preparation of micropatterned PNIPAAm hydrogels. (a) A PNIPAAm terpolymer film is spin-coated on a functionalized glass substrate and illuminated with a weak dose (0.28 J/cm^2) of collimated UV light (365 nm) to obtain an anchored, cross-linked polymer network. (b) Further UV illumination (3.92 J/cm^2) through a photolithography mask and (c) subsequent rinsing with ethanol leads to the formation of a PNIPAAm film with a defined pattern of shallow, weakly cross-linked areas. (d) Submersion in aqueous solutions creates a PNIPAAm hydrogel in which the weakly cross-linked areas swell more than the rest of the film and form a pillar pattern. (e) White-light confocal profilometry image of a dry structured PNIPAAm film. (f) Confocal laser scanning microscopy image (xz view) of the patterned PNIPAAm hydrogel, swollen in phosphate buffered saline (PBS) containing a small amount of rhodamine 6G that adsorbs to the gel (see text for details).

hydrogel layers is schematically shown in Figure 1. As a hydrogel-forming material, we used a poly(*N*-isopropylacrylamide)-based statistical terpolymer (PNIPAAm). Its backbone included 94% of NIPAAm units as a main component, approximately 5% of ionizable methacrylic acid units for increased solubility in water, and 1% hydrophobic benzophenone-based cross-linker (see the Supporting Information for the reaction).

The procedures for the synthesis of the PNIPAAm terpolymer and its processing into thin anchored hydrogel layers are well established in our laboratory and described in detail in the Methods.^{19–22} Briefly, a thin PNIPAAm film ($1.1 \pm 0.1 \mu\text{m}$ in the dry state) was spin-coated from an ethanol solution on glass substrates prefunctionalized with benzophenone silane. The film was illuminated with collimated UV light (Figure 1b) that lead to activation of the benzophenone groups on both the polymer chains and the glass surface and therefore to simultaneous cross-linking and anchoring of the PNIPAAm network.^{20,23} By tuning the exposure dose of the UV light, one can control the degree of cross-linking and thus the swelling ratio R_s of the PNIPAAm hydrogel films (see Figure S1 and Table S1 for details). To prepare micropatterned hydrogels, an initial homogeneous UV illumination of the PNIPAAm film at a low-energy dose (Figure 1a) that ensured anchoring and low-density cross-linking of the entire film was followed by further UV illumination through a photolithography mask (Figure 1b). The mask covered a square pattern of circles on the PNIPAAm film and protected them from further illumination and cross-linking. The noncovered parts were illuminated further, leading to the formation of a strongly cross-linked background area on the film. After the illumination, the PNIPAAm film was rinsed with ethanol, thus removing the non-cross-linked and non-anchored polymer chains. This resulted in the formation of a dry polymer film with shallow circular holes with defined diameters ordered in a precise square pattern (Figure 1c). The polymer network in these holes is less cross-linked than its surroundings, and upon swelling with water, it swells more creating a pattern of strongly swollen hydrogel pillars on a less swollen background (Figure 1d). A typical white-light confocal profilometry image of a dry patterned PNIPAAm film after rinsing with ethanol is shown in Figure 1e. The square pattern of round holes with a depth of $0.3 \mu\text{m}$ is clearly visible. In these weakly illuminated regions, more polymer chains were not cross-

linked and rinsed off by the ethanol. The rest of the film itself has a thickness of $1 \mu\text{m}$. Below the holes, a $0.7 \mu\text{m}$ thick layer of polymer remains. Figure 1f shows a confocal laser scanning microscopy (CLSM) image (xz view) of the same patterned PNIPAAm film after swelling in phosphate buffered saline (PBS). To enable CLSM imaging, a small amount of fluorescent rhodamine 6G molecules that preferably adsorb to the PNIPAAm due to hydrophobic interactions²² was added to PBS. The image reveals a pattern of strongly swollen ($R_s \approx 30$) hydrogel pillars on top of the less swollen ($R_s \approx 10$) background.

2.2. Formation of Monodisperse Giant Unilamellar Anchored Vesicles. GUAVs were prepared by hydration of a dry layer of lipids spread on the surface of a dry patterned PNIPAAm film (Figure 2). As a model membrane system, we used 1,2-dioleoyl-*sn*-glycero-3-phosphocholine (DOPC) and 1,2-dioleoyl-*sn*-glycero-3-phosphoserine (DOPS) in a 4:1 ratio. A small amount (0.5%) of Atto488-labeled 1,2-dioleoyl-*sn*-glycero-3-phosphoethanolamine (Atto488-DOPE) was added to enable confocal microscopy imaging. First, a lipid layer was deposited on top of a dry patterned PNIPAAm film by drop casting $30 \mu\text{L}$ of chloroform solution (1 g/L). The lipid solution spread over the entire surface of the patterned PNIPAAm film and the chloroform evaporated within minutes under ambient conditions. Afterward, the microscope-coverslip glass substrate supporting the PNIPAAm film was mounted on an Attofluor Cell Chamber (Thermo Fisher Scientific) with the lipid layer facing upward, and $600 \mu\text{L}$ of phosphate-buffered saline (PBS) was slowly added to the chamber. Within 5 min, the background gel swelled to a thickness of approximately $10 \mu\text{m}$ (that corresponds to $R_s \approx 10$) and the pillars to $20 \mu\text{m}$ ($R_s \approx 30$), and numerous giant vesicles formed. The experiments were performed at room temperature, $23 \text{ }^\circ\text{C}$.

Vesicle formation speed and mechanisms are comparable to that observed on PVA gels or agarose substrates.^{24,25} However, in contrast to these early works that used homogeneous substrates and thus the GUVs form randomly and have a very broad size distribution (Figure 2a), on the micropatterned PNIPAAm film, giant vesicles can form only on the weakly cross-linked and strongly swollen pillars (Figure 2b). Furthermore, the giant vesicles have a well-defined size determined by the pillars' diameter (Figure 2d). On the strongly cross-linked parts of the film, vesicle formation is

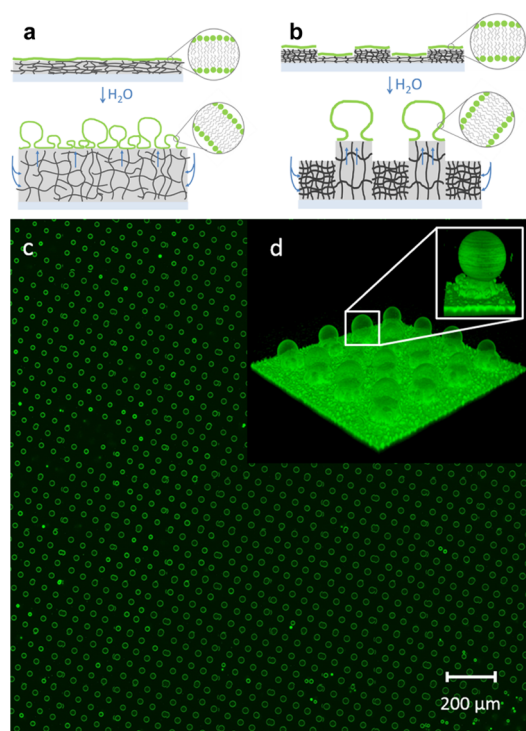


Figure 2. Formation of giant vesicles. Schemes of GUAVs forming (a) with various sizes on a homogenous hydrogel film and (b) with a defined size on the pillars of a micropatterned hydrogel film. A dry layer of lipids spread on the surface of a dry PNIPAAm gel is hydrated from water coming from below (blue arrows) and swelling the gel. (c) 2D CLSM image of an array of uniform GUAVs, prepared on a micropatterned PNIPAAm hydrogel. (d) 3D CLSM image of an array of 16 GUAVs zoomed in to a single pillar with one GUAV on top.

inhibited (see Figure S2 and the Supporting Information for details), and only very small vesicles grew in these areas. The 3D CLSM images in Figure 2d reveal that the lipids not only form vesicles on the top of the PNIPAAm hydrogel pillars but also partially penetrate into the polymer network. Thus, the unilamellar vesicles are immobilized on controlled positions, according to a predefined pattern that is a promising alternative to other immobilization methods.^{26,27} We name this new type of lipid vesicle system Giant Unilamellar Anchored Vesicles (GUAVs). Thousands of such uniformly sized GUAVs ordered in a predefined pattern (Figure 2c) can be prepared in a few minutes. Similar to the vesicles formed on PVA gels or agarose substrates,^{24,25} the anchored vesicles prepared on the micropatterned PNIPAAm hydrogels are unilamellar as indicated by the similar fluorescence brightness that they show on the CLSM images. The fact that in Figure 2c some smaller vesicles appear brighter than the rest is caused by the limited resolution of the shown image as demonstrated in Figure S3.

Furthermore, the size of the GUAVs can be easily controlled by tuning the diameter of micropatterned PNIPAAm pillars. This is demonstrated in Figure 3 that shows CLSM images of GUAVs formed on PNIPAAm films patterned with three different photolithography masks. The diameters of the nontransparent circles were 15, 30, and 50 μm . With diameters of 15.8 ± 3.1 , 30.9 ± 2.4 , and 46.1 ± 2.8 μm , the generated GUAVs closely match the sizes defined by the photolithography masks. Note that such a close correspondence of sizes cannot be determined only by the amount of lipids

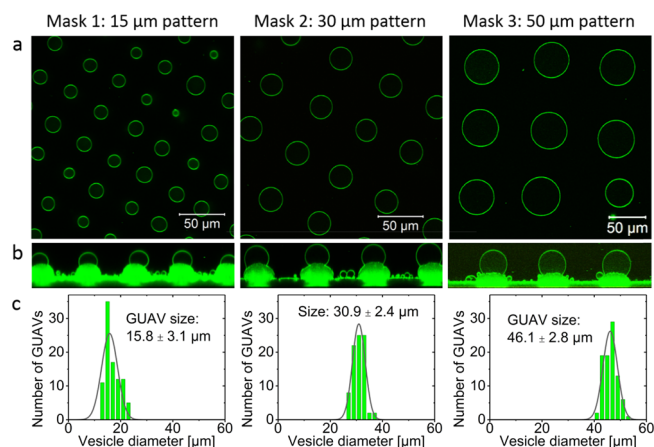


Figure 3. Controlling the vesicle size. GUAVs prepared by PNIPAAm gel-assisted swelling for three different mask/pattern sizes. (a) CLSM images (xy plane) of GUAVs, labeled with Atto488. (b) CLSM images (xz plane) of GUAVs. (c) Size distribution of the GUAV diameters. The histograms were obtained by measuring the diameters of roughly 90 GUAVs for each pattern. The lines represent a normal distribution fit that yielded the values of the average GUAV diameter and the respective standard deviation.

available on the pillar before swelling since there is a factor of four between the surface of a sphere and the surface of its two-dimensional projection; formation of a vesicle from a bilayer patch of radius R should result in a vesicle of radius $R/2$. For the GUAV technique, it is likely that the anchoring conditions of the bilayer on the pillar, as seen in Figures 2d and 3b, also play an important role in controlling the vesicle size.

The strategy developed in this paper relies on the differential swelling ratios between gel regions of high and low cross-linking densities. After swelling, the highly swollen regions of the gel appeared as pillars decorated with a giant vesicle. The hard regions surrounding the pillars did not lead to giant vesicle growth. Thus, the parameters of the pattern of the optical mask controlling the geometry of the high and low cross-linked regions translated directly into giant vesicle size and positioning. The method will allow preparing not only giant vesicles with monodisperse size but also more complex but well-defined mixtures of vesicles with different sizes anchored on predetermined positions. In particular, it could be useful to prepare arrays of GUAVs with sizes gradually changing, for example, between 50 μm and 5 μm , and study the effect of vesicle size in a single microscopy experiment.

Such an approach takes advantage of the anchoring of GUAVs after the swelling of the hydrogel film. While the detailed nature of this anchoring is not completely clear yet, most likely, it originates from hydrophobic attraction between the lipids and the hydrogel films. As discussed above, as the hydrogel-forming material, we used a statistical terpolymer (PNIPAAm) which backbone contains also 1% of hydrophobic benzophenone-based cross-linker units. In previous studies, we have found that the presence of these units leads to hydrophobic attraction between similar PNIPAAm hydrogels and partially hydrophobic molecules such as immunoglobulin²⁸ or rhodamine 6G.²² The existence of such attraction is also indicated by the fact that a large number of lipids are partitioned inside the swollen hydrogels as shown in Figure 3b. Furthermore, electrostatic interactions can also be present and eventually lead to systematic differences in the partitioning behavior of charged and uncharged lipids.

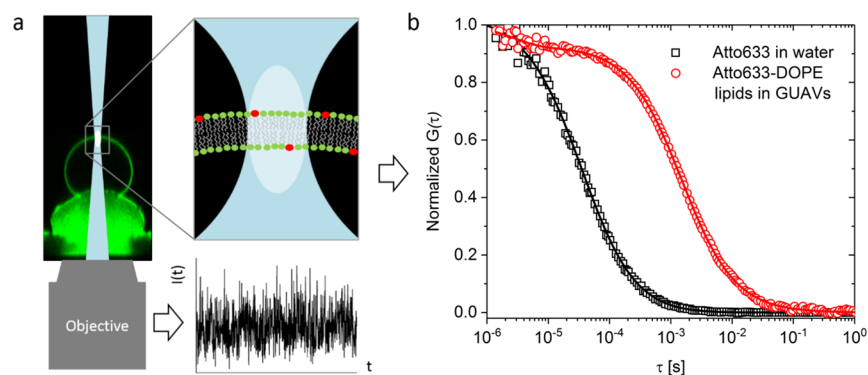


Figure 4. Lipid diffusion in the bilayer membrane of a GUAV measured by fluorescence correlation spectroscopy. (a) Schematic of the experiment. The fluorescence (green) of the Atto488-DOPE lipids present in the GUAV membrane at a 0.5% fraction is used to image the vesicles and position the confocal volume precisely at the lipid membrane. Next, excitation at 633 nm is used to excite the Atto633-DOPE lipids that are present at a low (0.01%) fraction suitable for FCS experiments. The temporal fluctuations of the detected fluorescence intensity $I(t)$ caused by the lateral diffusion of the Atto633-DOPE lipids (red) through the confocal volume are recorded and processed to an autocorrelation curve. (b) Normalized autocorrelation curve $G(\tau)$ measured for Atto633-labeled DOPE lipids diffusing in the bilayer membrane (red circles) and the corresponding fit (red solid lines) with a 2D diffusion model function. The autocorrelation curve measured for the reference dye used for calibration of the confocal volume, Atto633, freely diffusing in water (black squares) and the corresponding fit (black solid lines) with a 3D diffusion model function are also shown for comparison.

2.3. Lipid Mobility in the Bilayer Membrane of GUAVs. To demonstrate the advantages of anchored giant vesicles with respect to position control, we investigated the mobility of lipids by fluorescence correlation spectroscopy (FCS).^{29,30} Due to its high selectivity, sensitivity (down to a single-molecule level), and extremely small probing volume ($<1 \mu\text{m}^3$) that can be precisely positioned on the lipid membrane, FCS is uniquely suited for such studies.^{29,30} Here, we study the lateral diffusion of Atto633-DOPE (Atto633-1,2-dioleoyl-*sn*-glycero-3-phosphoethanolamine) lipids in the membrane of the GUAVs (Figure 4). Therefore, 0.01% of Atto633-DOPE was added to the standard lipid mixture used for the preparation of GUAVs. The GUAVs were first imaged with CLSM at 488 nm, the excitation wavelength of Atto488-DOPE lipids present in the membrane at the 0.5% fraction. Next, the confocal volume was positioned precisely at the lipid membrane on the “north pole” of a GUAV (Figure 4a), and FCS measurements were performed with the Atto633-DOPE lipids using an excitation wavelength of 633 nm. Due to the anchoring of the GUAVs, the lipid membrane position was stable with respect to the confocal volume, and thus FCS experiments could be performed over many minutes.

A typical FCS autocorrelation curve measured in this way is shown in Figure 4b together with the corresponding fit with an analytical function based on a single-component two-dimensional diffusion model.^{29,30} The fit yielded a value of $D = (1.01 \pm 0.14) \times 10^{-11} \text{ m}^2/\text{s}$ for the diffusion coefficient of Atto633-DOPE lipids. This value is in good agreement with the results of earlier FCS studies of labeled lipid diffusion in lipid GUVs.^{31–33}

2.4. Photo-Oxidation of the GUAV Membrane. The GUAV platform allows following simultaneously the physicochemical transformation of lipid bilayers on many vesicles. As an example, we studied lipid photosensitization.^{34–36} Photosensitizer erythrosine (50 μM) was added to phosphate buffered saline (PBS) and irradiated at 547 nm to create singlet oxygen that oxidizes the lipid bilayers.^{34,35} Under such conditions, membrane area changes are expected following the formation of hydroperoxides, the primary product of photosensitization.^{37–39} Therefore, we monitored the area

increase of the GUAVs equator as a function of the irradiation dose. For these particular experiments, an array of 9×9 GUAVs was chosen (Figure 5), but much larger numbers of

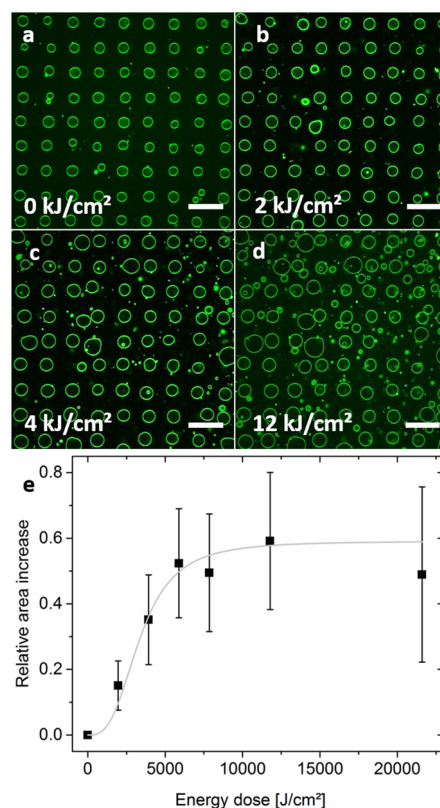


Figure 5. Photo-oxidation experiments on GUAVs. Confocal laser scanning images of the equator of GUAVs after illumination with different irradiation doses. (a) Before irradiation the GUAVs are uniform and completely round-shaped. With irradiating the photo-oxidizer erythrosine, the GUAVs become larger, deform, and move from their positions. (b–d) The effect increases with increasing dose. Scale bars are $50 \mu\text{m}$. (e) Area increase of the GUAV equator as a function of energy dose.

vesicles can be monitored depending on the target resolution. As the images show, the fate of each individual vesicle in the array can be easily monitored, and measurements such as the changes in the relative area of the equatorial plane (Figure 5e) can be straightforwardly performed by image analysis.

Variations in values of the area increase are intrinsic to this process and also seen in GUVs, as for instance reported in ref 38, although they are likely amplified here by heterogeneities in the anchoring conditions between the membrane and the gel.

3. CONCLUSIONS

We have shown here that the ability to spatially modulate the crosslinking density of a thin gel brings unprecedented size control in the gel-assisted formation of single-bilayer vesicles. By patterning the cross-linking density in thin gels of PNIPAAm, we have obtained essentially monodisperse giant anchored vesicles with a variation in diameters smaller than 10%.

The strategy developed in this paper relied on the differential swelling ratios between gel regions of high and low cross-linking densities. After swelling, the highly swollen regions of the gel appeared as pillars decorated with a giant vesicle, the hard regions surrounding the pillars did not lead to giant vesicle growth. This happened because the vesicle formation process is strongly dependent on the degree of cross-linking and the swelling ratio even for unstructured PNIPAAm gels (see Figure S2 and the Supporting Information for details). While a large number of vesicles with various sizes form on such gels, there is a general tendency that the average size and the fraction of large vesicles are decreasing gradually with the increase of cross-linking density (Figure S2). Thus, the parameters of the pattern of the optical mask controlling the geometry of the high and low cross-linked regions translated directly into giant vesicle size and positioning. The transferability from pattern design to giant vesicle properties is an intrinsic flexible powerful feature of the method, as it will allow preparing not only giant vesicles of a targeted size but also more complex but well-defined mixtures of different sizes with predetermined positions.

Indeed, contrary to gel-assisted growth with other polymer gels, the giant vesicles here remained attached to the substrate and positioned on the pillars. As a result, thousands of anchored, precisely positioned giant vesicles are formed upon simple addition of the solution to the dry patterned gel where lipid was spread. The anchoring is due to the lipid penetration into the dry and swollen gel, which changes the capillary boundary conditions between the bilayers and the substrate. Although the detailed structure of the anchoring region is likely to determine how well the interior of the GUVs is sealed with respect to different molecules, it does not compromise the purity of the formed GUVs since the gel is chemically cross-linked. It is important to underline that the stability of this giant vesicle platform is insured also by the chemical cross-linking of the gel film to the substrate, resulting in a very robust formation and observation platform for GUVs.

Physical measurements performed on GUVs revealed also the possibilities offered by this platform with respect to position control and parallel measurements under a microscope. FCS measurements could be performed under very stable conditions for several minutes, providing lipid diffusion coefficients in agreement with values from the literature. Photosensitization of the vesicles was also easily achieved, and the resulting transformations could simultaneously be followed

and qualitatively evaluated on many vesicles. Excitingly, these achievements are a key step toward the development in a near future of automated measurements under an optical microscope on massive arrays of biomimetic lipid membranes.

4. MATERIALS AND METHODS

4.1. 4-Methacryloyloxybenzophenone (MABP). Ten grams (50 mmol) of 4-hydroxybenzophenone was dissolved in 100 mL of dichloromethane (DCM), the mixture was cooled in an ice bath, and a solution of 5.1 mL (53 mmol) of methacryloyl chloride and 7.7 mL (56 mmol) of triethylamine in 20 mL of dry DCM was added dropwise. The reaction was stirred at room temperature for 4 h. The solvent was evaporated, and the residue was dissolved in diethyl ether. The nonsoluble triethylammonium salt was removed by filtration. The organic phase was washed with water three times and afterward dried over Na_2SO_4 . The solvent was evaporated, and the crude product was chromatographed over DCM/hexane (7:3). The product was recrystallized from a mixture of DCM and hexane (2:8).

4.2. Functionalization of the Glass Substrates. Round microscope cover slides (diameter: 25 mm, thickness: 150 μm) were used as substrates for the polymer films. The glass slides were cleaned with 2% Hellmanex solution (Hellmanex II, Hellma GmbH, Müllheim), ultrapure water (Milli-Q water, 18.2 M Ω cm), and twice with ethanol (each time with 15 min sonication in the corresponding solvent/solution). Afterward, the glass slides were stored for at least 24 h in 6% benzophenone triethoxysilane ethanol solution under argon in the dark. Then, the slides were washed with ethanol and dried under vacuum for 1 h at 50 °C.

4.3. Poly(*N*-Isopropylacrylamide)-Based Terpolymer. Ten grams (88 mmol) of *N*-isopropylacrylamide (NIPAAm) (recrystallized from toluene/hexane, 1:1), 380 mg (0.37 mL, 4.4 mmol) methacrylic acid (MAA) (distilled before use), and 235 mg (0.88 mmol) 4-methacryloyloxybenzophenone (MABP) were dissolved in 68 mL dioxane. Argon was flown through the solution for 1 h. Sixty-seven milligrams (0.41 mmol) of azobisisobutyronitrile (AIBN) was added to the solution, and the reaction was stirred at 60 °C under argon for 48 h. For purification, the reaction solvent was evaporated, and the product precipitated from methanol in ice cold diethyl ether. The molecular weight was $M_w = 220$ kg/mol, and the polydispersity index was $\text{PDI} = 1.55$, as obtained from gel permeation chromatography. See Scheme S1 for the synthetic route.

4.4. Polymer Template. Polymer films were prepared from 10 wt % PNIPAAm terpolymer solution in ethanol. The solution was spin-coated at room temperature onto the prefunctionalized round microscope glass substrates at 2500 rpm for 30 s. After spin-coating, the samples were solvent-vapor-annealed for 1 h in ethanol vapor and afterward temperature-annealed for 1 h at 170 °C in vacuum. Then, the samples were dried for 24 h at 50 °C under vacuum. The polymer was cross-linked and anchored to the glass substrate by irradiation with UV light (365 nm) using an LED (LCS-0365-07-22 High-Power LED Collimator Source, 365 nm, 7 W, 22 mm aperture, type B). For micropatterning, different photolithography masks with appropriate structure were positioned onto the samples.

The total irradiation energy dose for cross-linking was 4.2 J/cm², 0.28 J/cm² before and 3.92 J/cm² after adding the photolithography mask. These values are estimated based on a

calibration experiment in which the intensity of UV light versus the LED current was measured without any photolithography mask between the LED and optical power meter. Thus, the real energy dose reaching the patterned PNIPAAm films can be lower. Subsequently, the samples were rinsed with pure ethanol and dried at 50 °C for 1 h under vacuum.

4.5. Giant Unilamellar Anchored Vesicle (GUAV)

Formation. Phospholipids were purchased from Sigma-Aldrich as powder. 1,2-Dioleoyl-*sn*-glycero-3-phosphocholine (DOPC) and 1,2-dioleoyl-*sn*-glycero-3-phosphoserine DOPS were dissolved in chloroform ($c = 1$ g/L). As a fluorescent marker, Atto488-labeled 1,2-dioleoyl-*sn*-glycero-3-phosphoethanolamine (Atto488-DOPE) was used and dissolved in dichloromethane and methanol (8:2) ($c = 1$ g/L).

Lipid solutions were stored at -20 °C before use. The final lipid solution for GUAV formation was prepared from the DOPC solution with 20% DOPS and 0.5% Atto488-DOPE. The lipid solution (30 μ L) was added to the polymer sample. After evaporation of chloroform, 600 μ L PBS (phosphate buffered saline, pH 7.4) was used to grow GUAVs.

4.6. Confocal Laser Scanning Microscopy. Confocal laser scanning microscopy (CLSM) experiments were performed with a commercial setup (Carl Zeiss, Jena, Germany), consisting of an inverted microscope model Axiovert 200, the module LSM510, and a Zeiss C-Apochromat 40 \times /1.2 W water immersion objective. The Atto488-labeled lipids were excited with an argon ion laser with a wavelength of 488 nm. The samples were measured in Attofluor cell chambers at room temperature.

4.7. Determination of the Lipid Diffusion Coefficient via Fluorescence Correlation Spectroscopy. To the mixture of phospholipids for the GUAV formation, 0.01% Atto633-labeled DOPE was added, and the GUAVs were prepared as described above. FCS experiments were performed on an LSM 880 (Carl Zeiss, Jena, Germany) setup. Excitation laser light was focused on the samples using a Zeiss C-Apochromat 40 \times /1.2 W water immersion objective. The emission was collected with the same objective and, after passing through a confocal pinhole, directed to a spectral detection unit (Quasar, Carl Zeiss). In this, unit emission is spectrally separated by a grating element on a 32-channel array of GaAsP detectors operating in a single-photon counting mode.

An argon laser ($\lambda = 488$ nm) was used to excite the fluorescence of the Atto488-DOPE lipids present in the GUAVs membrane at the 0.5% fraction and thus image the vesicles and position the confocal volume precisely at the lipid membrane. Next, a HeNe laser ($\lambda = 633$ nm) was used for excitation of Atto633-labeled lipids, and emission in the range from 650 to 696 nm was detected with a QUASAR detection unit. An Attofluor metal chamber was used as a sample cell. For each sample, 10 measurements (30 s each) were performed. Obtained experimental autocorrelation curves were fitted with a theoretical model function for a 2D diffusion, yielding the diffusion coefficient of the Atto633-labeled lipids in the bilayer. Calibration of the size of the confocal volume was done by recording autocorrelation curves for a reference dye with a known diffusion coefficient, that is, Atto633 freely diffusing in water.

4.8. Photo-Oxidation. Erythrosine was purchased from Sigma-Aldrich as a powder and was diluted in phosphate buffered saline (PBS, pH 7.4) to a concentration of 50 μ M. For imaging, we used an LSM 880 confocal laser scanning

microscope (Carl Zeiss, Jena, Germany) equipped with a Zeiss C-Apochromat 40 \times /1.2 W water immersion objective. Atto488-labeled DOPE lipids were excited by an argon ion laser with a wavelength of 488 nm, and their emission in the range from 500 to 550 nm was detected with the QUASAR detection unit. For irradiation of the photo-oxidizer erythrosine, we used the microscope-attached mercury lamp (HXP 120 C, FSet43wf). Image analysis was performed with the software ImageJ.

■ ASSOCIATED CONTENT

Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acsomega.9b00912.

Swelling ratios and polymer fractions of the PNIPAAm hydrogel versus illumination energy dose; CLSM images of GUVs, formed on homogenous PNIPAAm hydrogel films; scheme of the PNIPAAm terpolymer synthetic route (PDF)

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Funding

This work was financially supported by the DFG (no. SFB 1066, Q2) and HFSP (no. RGP0013/2015).

Notes

The authors declare no competing financial interest.

■ ACKNOWLEDGMENTS

We thank Prof. Ulrich Jonas for the helpful discussions and Gunnar Kircher for his support with the chemical synthesis. We acknowledge the financial support by the DFG (no. SFB 1066, Q2) and HFSP (no. RGP0013/2015). C.M.M. acknowledges Max-Planck-Institut für Polymerforschung for their hospitality.

■ ABBREVIATIONS

DOPC: 1,2-dioleoyl-*sn*-glycero-3-phosphocholine; DOPE: 1,2-dioleoyl-*sn*-glycero-3-phosphoethanolamine; DOPS: 1,2-dioleoyl-*sn*-glycero-3-phosphoserine; CLSM: confocal laser scanning microscopy; FCS: fluorescence correlation spectroscopy; GU(A)V: giant unilamellar (anchored) vesicle

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Supporting Information

Preparation of monodisperse giant unilamellar anchored vesicles using micro-patterned hydrogel substrates

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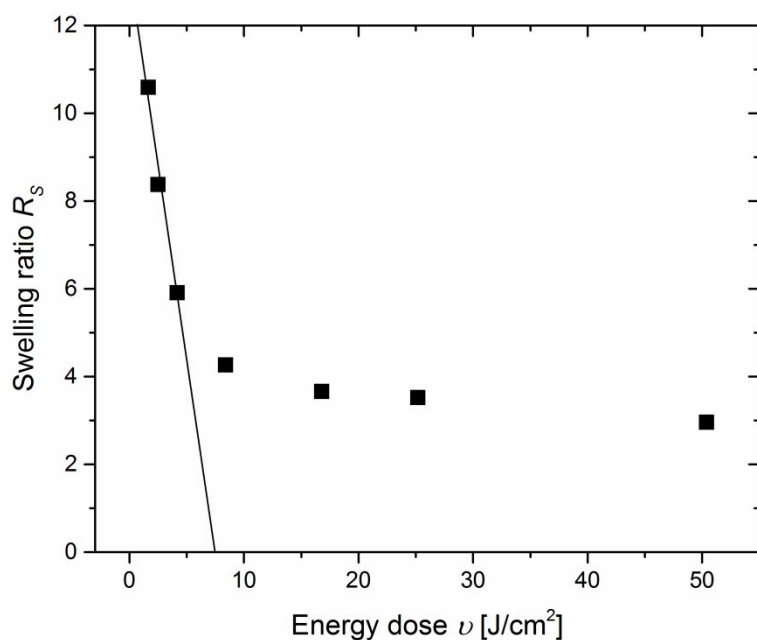


Figure S1. Swelling ratio R_s of the PNIPAAm terpolymer hydrogel films vs. energy dose ν in the cross-linking process.

Table S1. Swelling ratio R_S and polymer volume fraction ϕ of PNIPAAm hydrogel films prepared with different cross-linking energy doses. Films were fully swollen in ultrapure water.

Energy dose ν [J/cm ²]	Swelling ratio R_S	Polymer volume fraction ϕ
1.7	10.6	0.09
2.5	8.3	0.12
4.2	5.9	0.17
8.40	4.3	0.23
16.8	3.7	0.27
25.2	3.5	0.29
50.4	3.0	0.33

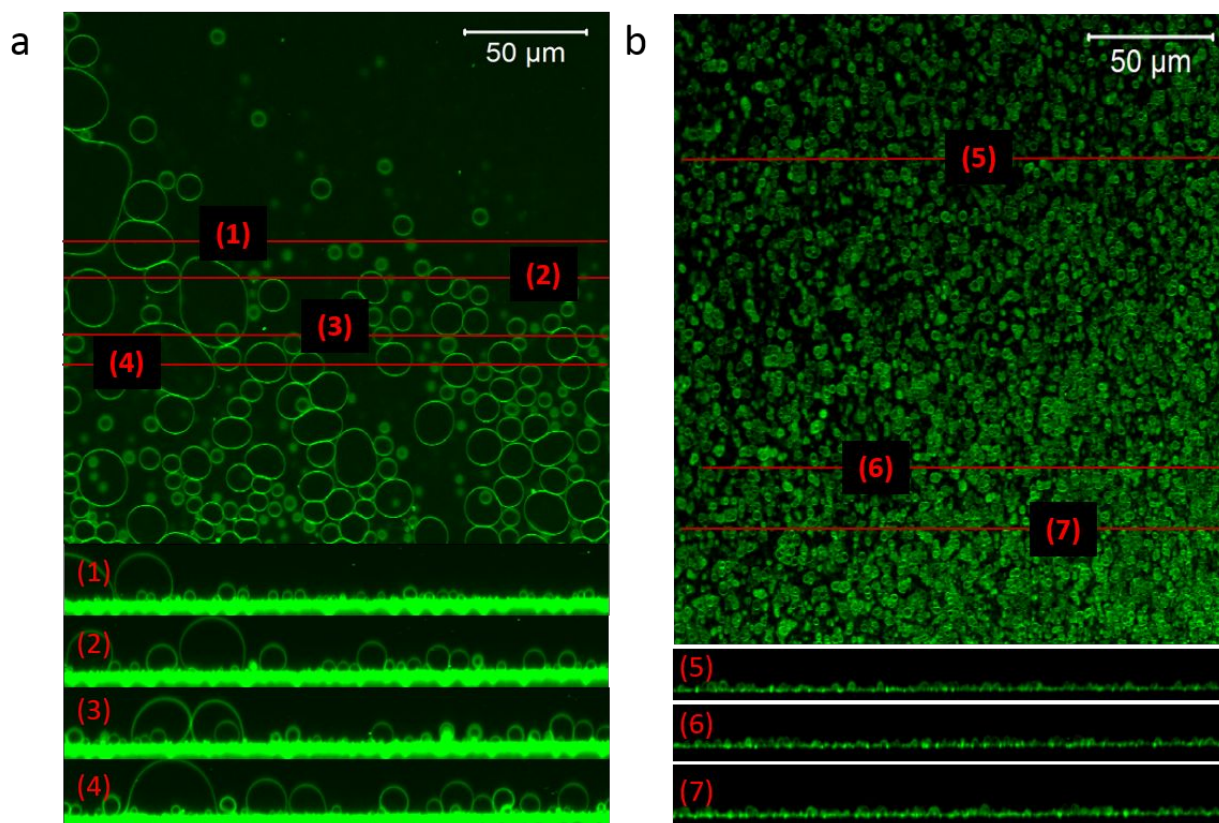
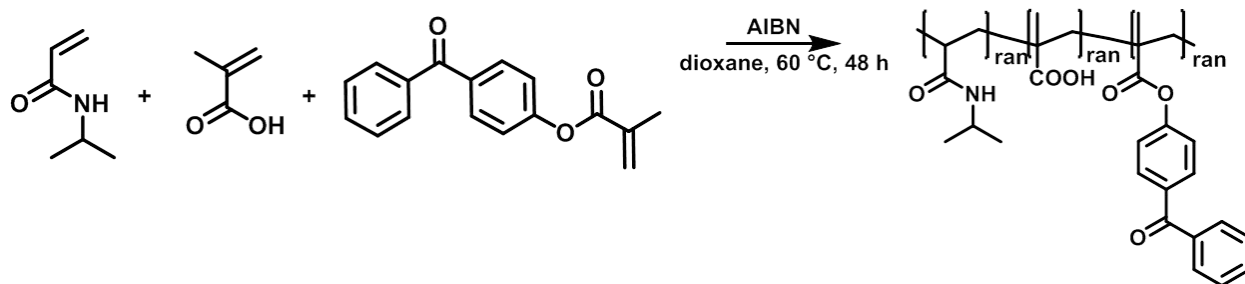


Figure S2. CLSM images of GUVs, formed on homogenous PNIPAAm hydrogel films with different crosslinking density. (a) Film cross-linked with an energy dose of 2 J cm⁻². Resulting GUV diameters are between 3 μm and 40 μm. x-z-plane images were taken at several positions (1)-(4). (b) Film cross-linked with an energy dose of 60 J cm⁻². Resulting GUV diameters are between 1 μm and 3 μm. x-z-plane images were taken at several positions (5)-(7).



Scheme S1. Synthetic route for preparing the PNIPAAm terpolymer.

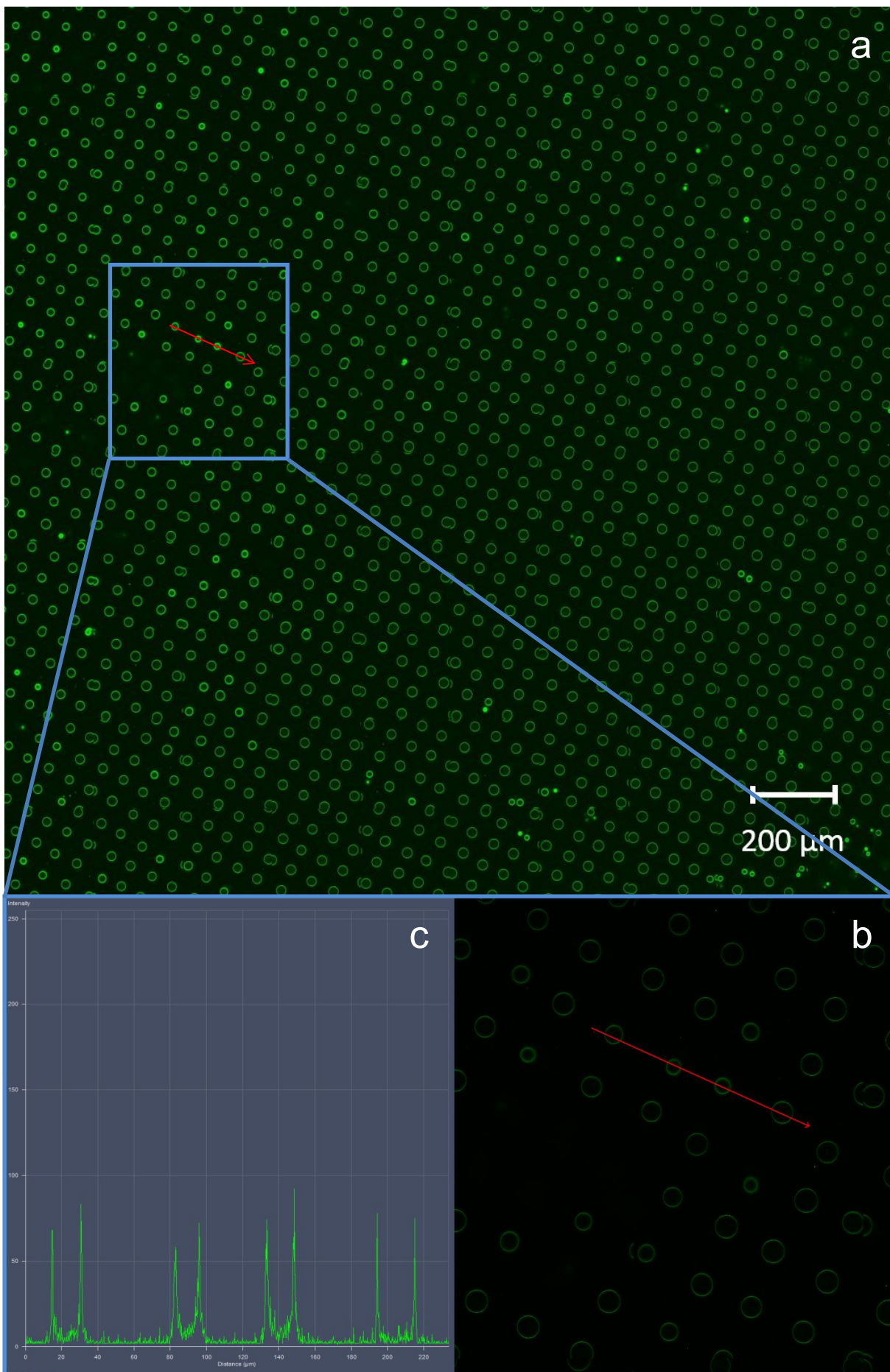


Figure S3. (a) 2D CLSM image of a GUAVs array, prepared on a micro-patterned PNIPAAm hydrogel (as on Figure 2c in the main text). (b) Zoomed part of the image and (c) the corresponding intensity profile, confirming that the vesicles are unilamellar. Some smaller vesicles in (a) appear brighter due to limited number of pixels in the image.